




## Article

# Impact of Portable Radiometers on Irradiance Measurements of LED Photocuring Units

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## Abstract

**Purpose:** The aim of this in vitro study was to evaluate the influence of different models of commercially available portable dental radiometers on the measurement of light irradiance emitted by light-emitting diode (LED) photocuring units. **Materials and Methods:** Eight LED photocuring units, all emitting light in a single-wavelength spectrum, were tested. Light irradiance (mW/cm<sup>2</sup>) was measured using six portable dental radiometers: four digital models (D1–D4) and two analog models (A1, A2). Digital model D1 was used as the reference (control). All measurements were conducted under standardized conditions, and each LED–radiometer combination was tested in triplicate. Data were analyzed using Sigma Plot 12.0 (Palo Alto, CA, USA) to verify the assumptions of normality and homogeneity of variances. A one-way analysis of variance (ANOVA) was used to assess the effect of the radiometer model on irradiance values, followed by Tukey’s post hoc test for multiple comparisons. The significance level was set at  $\alpha < 0.05$ . **Results:** No statistically significant difference in irradiance was found between D1 (control) and D2. However, significantly lower values were recorded with A2, while D3, D4, and A1 produced significantly higher irradiance values compared to the control ( $p < 0.05$ ). **Conclusion:** Irradiance measurements can vary significantly depending on the radiometer model used. Clinicians should be aware of this variability and are encouraged to regularly check the irradiance of the light-curing units used in daily practice, ensure their proper maintenance, and implement periodic monitoring to maintain effective clinical performance.

**Keywords:** dental materials; dental radiometers; dentistry; equipment maintenance; irradiance measurement; LED curing units; light curing; light-curing devices; light-curing materials; photopolymerization



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## 1. Introduction

Light-curing units (LCUs) are essential tools in modern dental practice due to the widespread use of resin-based materials that require light-induced polymerization to harden

and achieve functional stability [1]. Among these LCUs, light-emitting diode (LED) devices have become the most common, owing to their high energy efficiency, spectral precision, and reduced heat generation compared to older technologies such as quartz–tungsten–halogen units [2–4]. LED LCUs typically emit light in the range of 380–550 nm, targeting photoinitiators like camphorquinone, which is widely used in dental composites [5].

The effectiveness of light curing is a critical determinant of the degree of conversion (DC) of resin monomers into a stable polymer network. A high DC not only improves mechanical performance and clinical durability but also minimizes the release of unreacted monomers, which are associated with cytotoxicity and inflammatory responses in the surrounding tissues [6,7]. Thus, photocuring quality directly impacts both the physical integrity and biocompatibility of dental restorations, making irradiance a key parameter for clinicians and researchers alike [8].

To ensure optimal polymerization, it is important to regularly verify the output of LCUs using dental radiometers. These devices measure the spectral irradiance (power per unit area) emitted by a curing light and help detect device degradation over time [9]. Portable radiometers—available in various analog and digital models—are commonly used for this purpose, typically incorporating a photodiode sensor that converts light energy into electrical signals [5].

However, recent studies have shown that discrepancies exist between the irradiance values claimed by LCU manufacturers and those measured by radiometers in clinical settings [4]. Furthermore, the accuracy and consistency of different radiometer models vary significantly, which may lead to misleading results and affect clinical decision-making, such as the selection of a light-curing unit or the evaluation of whether its irradiance is sufficient to ensure the proper polymerization of resin-based materials. For example, a recent study found that even commercially available radiometers from reputable brands yielded variable irradiance measurements under identical conditions [10].

Given this variability, the aim of the present study was to evaluate and compare the irradiance measurements of different commercially available portable dental radiometers using the same LED LCU. The null hypothesis tested was that no significant differences in irradiance measurements would be observed across the tested radiometers. The alternative hypothesis is that there will be significant differences in the light irradiance measurements when the same PU is analyzed with different radiometers.

## 2. Materials and Methods

### 2.1. Study Design

An in vitro study was carried out. A total of 8 LEDs with monowave PUs were evaluated (Table 1 and Figure 1). All devices were used with 100% charged batteries and it was verified that the fiber tip of the unit was clean, without scratches or fractures. The units were set for 20 s, using the standard cure intensity mode. Except for D1, the radiometers used in this study were not brand new; however, they had been handled with care and stored under appropriate conditions. Prior to the study, all devices were verified for consistent readings through repeated measurements under controlled conditions. As no relevant discrepancies or fluctuations were observed, we considered them reliable for comparative evaluation. Among the devices tested, the Bluephase Meter II (Radiometer D1) was used as the reference or control device due to its reported accuracy and reliability in previous studies. Notably, this radiometer was brand new and had not been used in any prior experiments or clinical settings, which further supports its role as a reference standard for the comparison.

For all irradiance measurements, the light-curing unit was fixed in a custom-made acrylic support to ensure a stable position and a perpendicular orientation between the curing light tip and the radiometer sensor surface were maintained. Each radiometer

was placed on a flat, non-reflective surface, and measurements were taken without any external light interference. The distance between the curing light and each radiometer was standardized by direct contact with the sensor area, as recommended by the manufacturers. This setup minimized variability and allowed for reproducible measurement conditions.

**Table 1.** The characteristics of the polymerization units used in the present study.

	Brand (Group Code)	Model	Manufacturer	Tip Diameter (mm)	Intensity Declared by the Manufacturer (mW/cm <sup>2</sup> )	Batch
1	Woodpecker (W1)	LED-H	Guilin Woodpecker Medical Instrument; Guilin, China.	8.0	850–1000	L1341355H
2	Woodpecker (W2)	LED-H	Guilin Woodpecker Medical Instrument; Guilin, China.	8.0	850–1000	H12050071A
3	Woodpecker (W3)	LED-H	Guilin Woodpecker Medical Instrument; Guilin, China.	8.0	850–1000	L1560597H
4	Monitex (M1)	BlueLEX LD-106	MONITEX Industrial Company; New Taipei City, Taiwan.	8.0	1000	13L03778
5	Monitex (M2)	BlueLEX LD-106	MONITEX Industrial Company; New Taipei City, Taiwan.	8.0	1000	13L03776
6	Coxo (C1)	DB-686-1b	Foshan COXO Medical Instrument; Foshan, China.	8.0	1200	00310201409A
7	Coxo (C2)	DB-686-1b	Foshan COXO Medical Instrument; Foshan, China.	8.0	1200	00310201409A
8	Gnatus (G)	Optilight Max	Gnatus; San Paolo, Brazil.	8.0	1200	15070000046

All measurements were conducted in a light-controlled room to avoid interference from ambient illumination. The room temperature was maintained between 22 and 24 °C throughout the experiment.

Light irradiance (mW/cm<sup>2</sup>) was evaluated by using different portable dental radiometers (Figure 2 and Table 2). The evaluation was carried out at the same time by a single operator. Before measurements, the PU was fixed, allowing the tip to maintain a direct contact with the radiometer sensor. Three measurements per PU were taken and recorded. For the Bluephase Meter II radiometer, PU tip diameters were measured, and the value was recorded on the radiometer, as indicated by the manufacturer. It should be noted that new batteries were used in all radiometers for the measurements.

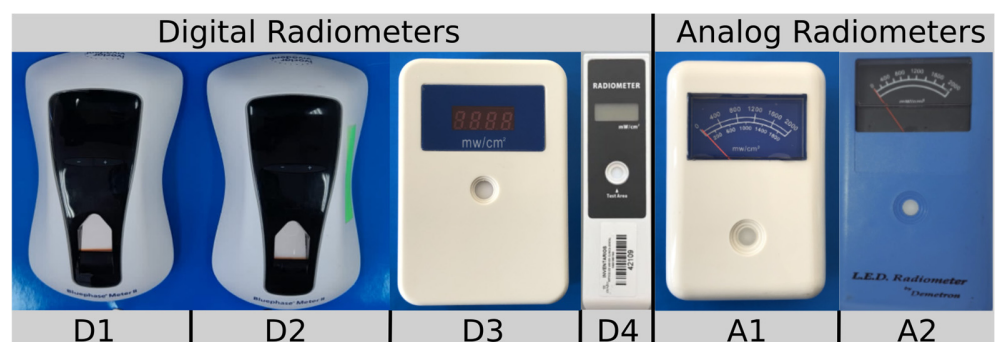
**Table 2.** The characteristics of the radiometers used in this work.

Brand (Group Code)	Manufacturer	Action Mode *	Spectral Range (nm)	Irradiance Range	Declared Accuracy	Batch
Bluephase Meter® II ** (D1)	Ivoclar-Vivadent; Schaan, Liechtenstein	Digital	380–550	300–12,000	±10%	1300003059
Bluephase Meter® II (D2)	Ivoclar-Vivadent; Schaan, Liechtenstein	Digital	380–550	300–12,000	±10%	1310001077
LVCHEN LED Light Meter (D3)	Generic product	Digital	N/S ***	N/S ***	N/S ***	N/S ***
Radiometer (D4)	Generic product	Digital	N/S ***	N/S ***	N/S ***	N/S ***
Analogical Radiometer (A1)	Generic product	Analogical	N/S ***	N/S ***	N/S ***	N/S ***
Kerr by Demetron (A2)	Kerr Dental; Brea, CA, EUA	Analogical	400–500	<2000	±5%	N/S ***

\* The mechanism by which the intensity is recorded in mW/cm<sup>2</sup>, which can be digital or analog. \*\* A second Bluephase Meter® II model was used as a control group. This product is new. \*\*\* N/S: NOT SPECIFY.



**Figure 1.** The light-curing units used.



**Figure 2.** The radiometers used in the study: D1—(control); D2—Bluephase Meter II; D3—LVCHEN LED Light Meter; D4—Radiometer LED; A1—Analogical Radiometer; and A2—Kerr Radiometer by Demetron.

## 2.2. Statistical Analysis

The data were analyzed using Sigma Plot 12.0 (Palo Alto, CA, USA) to verify the assumptions of normal distribution and variance homogeneity. The radiometer factor on the light irradiance was assessed through a one-way analysis of variance (ANOVA). Tukey's post hoc test was applied for multiple comparisons. In all analyses, the significance level was established at  $\alpha < 0.05$ .

## 3. Results

The irradiance values measured for each light-curing unit varied significantly depending on the radiometer used (one-way ANOVA,  $p < 0.05$ ).

For instance, in the case of the W1 curing unit, irradiance values ranged from  $410 \pm 20 \text{ mW/cm}^2$  (A2) to  $1361 \pm 20 \text{ mW/cm}^2$  (D4). The reference device D1 recorded  $500 \pm 10 \text{ mW/cm}^2$ , showing statistically significant differences compared to D3, D4, A1, and A2 ( $p < 0.05$ ).

Similar variations were observed for other curing units. For W3, values ranged from  $640 \pm 20$  mW/cm<sup>2</sup> (A2) to  $1790 \pm 20$  mW/cm<sup>2</sup> (A1). Although D1 and D2 provided similar values ( $860 \pm 10$  mW/cm<sup>2</sup> and  $870 \pm 10$  mW/cm<sup>2</sup>, respectively), significant differences were found when compared to D3, D4, A1, and A2.

The highest irradiance value recorded in the study was  $1990 \pm 20$  mW/cm<sup>2</sup> (D3, for unit C1), while the lowest was  $410 \pm 20$  mW/cm<sup>2</sup> (A2, for unit W1).

These results confirm that the same light-curing unit can yield significantly different irradiance values depending on the radiometer used. This highlights the variability among commercially available radiometers. The lowercase letters in Table 3 indicate statistically significant differences between devices (Tukey's post hoc test,  $p < 0.05$ ).

**Table 3.** The average intensity values (in mW/cm<sup>2</sup>) and standard deviation obtained after measurement with the radiometers.

Photocuring Units		Radiometers					
		D1	D2	D3	D4	A1	A2
1	W1	500 ( $\pm 10$ ) <sup>d</sup>	520 ( $\pm 10$ ) <sup>d</sup>	740 ( $\pm 20$ ) <sup>c</sup>	1361 ( $\pm 20$ ) <sup>a</sup>	990 ( $\pm 20$ ) <sup>b</sup>	410 ( $\pm 20$ ) <sup>e</sup>
2	W2	560 ( $\pm 10$ ) <sup>d</sup>	560 ( $\pm 10$ ) <sup>d</sup>	740 ( $\pm 20$ ) <sup>c</sup>	1428 ( $\pm 20$ ) <sup>a</sup>	990 ( $\pm 20$ ) <sup>b</sup>	490 ( $\pm 20$ ) <sup>e</sup>
3	W3	860 ( $\pm 10$ ) <sup>d</sup>	870 ( $\pm 10$ ) <sup>d</sup>	1640 ( $\pm 20$ ) <sup>b</sup>	1576 ( $\pm 20$ ) <sup>c</sup>	1790 ( $\pm 20$ ) <sup>a</sup>	640 ( $\pm 20$ ) <sup>e</sup>
4	M1	1020 ( $\pm 10$ ) <sup>d</sup>	1020 ( $\pm 10$ ) <sup>d</sup>	1490 ( $\pm 20$ ) <sup>c</sup>	1514 ( $\pm 20$ ) <sup>b</sup>	1590 ( $\pm 20$ ) <sup>a</sup>	690 ( $\pm 20$ ) <sup>e</sup>
5	M2	970 ( $\pm 10$ ) <sup>d</sup>	980 ( $\pm 10$ ) <sup>d</sup>	1690 ( $\pm 20$ ) <sup>a</sup>	1544 ( $\pm 20$ ) <sup>b</sup>	1390 ( $\pm 20$ ) <sup>c</sup>	690 ( $\pm 20$ ) <sup>e</sup>
6	C1	1220 ( $\pm 10$ ) <sup>d</sup>	1220 ( $\pm 10$ ) <sup>d</sup>	1990 ( $\pm 20$ ) <sup>a</sup>	1658 ( $\pm 20$ ) <sup>c</sup>	1890 ( $\pm 20$ ) <sup>b</sup>	1000 ( $\pm 20$ ) <sup>e</sup>
7	C2	920 ( $\pm 10$ ) <sup>d</sup>	910 ( $\pm 10$ ) <sup>d</sup>	1440 ( $\pm 20$ ) <sup>c</sup>	1550 ( $\pm 20$ ) <sup>b</sup>	1590 ( $\pm 20$ ) <sup>a</sup>	780 ( $\pm 20$ ) <sup>e</sup>
8	G	1160 ( $\pm 10$ ) <sup>c</sup>	1160 ( $\pm 10$ ) <sup>c</sup>	1240 ( $\pm 20$ ) <sup>b</sup>	1278 ( $\pm 20$ ) <sup>a</sup>	590 ( $\pm 20$ ) <sup>e</sup>	980 ( $\pm 20$ ) <sup>d</sup>

Different lowercase letters indicate the presence of statistically significant differences between radiometers for each light-curing unit ( $p < 0.05$ ), as determined by one-way ANOVA followed by post hoc Tukey tests.

#### 4. Discussion

In the present work, the light irradiance of different light-emitting diode (LED) photocuring units was measured using portable digital and analog dental radiometers available on the market, comparing the variation between them. The results obtained suggest that the intensity values depend on the type and model of radiometer used. Therefore, we can say that the null hypothesis has been rejected.

The radiometers included in this study were selected based on their widespread use in dental practice and their representation of different measurement technologies (analog and digital). This choice aimed to provide a realistic comparison reflective of commonly available options for clinicians. Although the devices were not new, their consistent performance during preliminary checks supports the validity of the recorded measurements.

The international standardization of organization (ISO) 10650 standard [11] suggests the use of a laboratory meter to quantify the radiant energy output to measure PU irradiance [11]. This type of equipment is not usually available in dental offices. Instead, some researchers use portable dental radiometers to monitor PU irradiance [9,12]. Bluephase Meter II has been suggested as a commercial control because the irradiance values measured are similar to those reported by laboratory radiometers, and because it shows less variation in the readings than other hand-held radiometers available in the market [12,13], as confirmed by the results obtained in this study. One explanation for its consistent readings could be due to the fact that Bluephase Meter II allows for the measurement of the UP tip diameter for the final irradiance calculation.

In the present study, no differences were observed between the irradiance of the different PUs when evaluated by Bluephase Meter II: D1 (control) and D2. On the other hand, significantly lower values were reported in some units when evaluated using the analog



radiometer A2, and significantly higher values when using the radiometers D3, D4, and A1 in comparison with the control. Various studies have reported a similar behavior [12,13].

Irradiance measurements of portable dental radiometers are affected by the tip diameter, light-beam profile, and emission spectrum [14]. The lack of precision in radiometers lies in two factors; first, some dental radiometers only test a small portion of the UP light emission surface, which subsequently is used as a sample to predict the total irradiance [15]. On the other hand, the light-beam profile of most PUs is not always the same, and the irradiance can significantly vary in different zones of the light-emitting tip. For this reason, the radiometer reading can vary greatly in the same PU, depending on what portion of the light emission tip is being tested [14,16]. Another reason why radiometers tend to record different readings is that many of them are not very sensitive to certain wavelengths; this makes it difficult to obtain an exact measurement, since PUs can emit light in a wide spectrum [17].

Also, commercial radiometers differ in the way they convert light into electrical current [16,18]; for this reason, there are challenges when measuring the irradiance supplied by different PUs [19]. In addition to this, the sensor diameter of the radiometers can vary, and often it is different to the diameter of the PU tip [20]. The size and shape of the sensor could modify the amount of light that actually reaches the detector. In fact, if the tip of the PU is moved above the sensor, a wide fluctuation in irradiance values can be observed [21].

When measuring the irradiance of a PU unit, the distance between the light beam and the sensor is relevant and must be 0 mm [22]. In addition, older halogen PUs needed light filtering, and this could reduce the irradiance at certain wavelengths. Generally, LED units manage to limit the wavelength spectrum in which they emit light, so this filtering is usually minimal. It should be noted that some photoinitiators used in the most current composite resins do not have the same excitation peak in terms of the required wavelength compared to the most used commercial photoinitiator, which is camphorquinone, and this wavelength may not be included in the irradiance value reported by the radiometer [23].

According to the results obtained, irradiance values vary between different radiometers. Since photoactivation time is irradiance dependent, these variations could have clinical repercussions [22]. An example of this is the W1 unit; when measured with the control radiometer (D1), this PU emits an irradiance of  $500 \text{ mW/cm}^2$ , so its photoactivation time should be 40 s; on the other hand, when evaluated with the D4 radiometer, it emits an irradiance of  $1361 \text{ mW/cm}^2$ , so its photoactivation time should be 20 s.

The display, especially of those digital radiometers, provides an accurate reading—for example, an intensity value of  $927 \text{ mW/cm}^2$ . However, this number can often differ by up to  $\pm 20\%$  from the actual correct value of the unit even when measured by a radiometer with the highest precision. The irradiance from 12 LED light-curing units was measured using five brands of dental radiometers [9]. On the other hand, in analog radiometers, a needle indicates the intensity value emitted by the unit, so the reading does not always refer to a precise value but rather an approximation. This has led to the belief that digital radiometers are the most appropriate [13]. For all of the above, we can say that currently the reference instruments for measuring radiant output continue to be laboratory type [24].

Despite the limitations of dental portable radiometers, they can be useful for clinicians to monitor any changes in the irradiance that may occur over time. The differences in size and costs for their acquisition are also worth mentioning. Most researchers recommend periodically monitoring the irradiance of the PU with a radiometer, documenting the results on a spreadsheet. Even if the current number is not accurate, the clinician is able to notice when there is a significant drop in irradiance and send it for repair or replacement [25].

The results expressed in this study must be interpreted with caution, since the measurements were carried out by analyzing the radiometers available on the market, and

not all existing types and models were included. The selection was based on the most commonly used devices available at the time. Moreover, despite the fact that a single-time measurement may not fully capture variations in performance over time, longitudinal assessments would provide valuable insights into device consistency and reliability.

Moreover, another limitation is related to the absence of manufacturer-reported data on spectral sensitivity and measurement accuracy for several radiometers, as noted in Table 2. Since radiometer performance is highly dependent on the similarity between the device's spectral sensitivity and the emission spectrum of the light-curing unit, this missing information introduces a degree of uncertainty regarding the absolute validity of some measurements. In addition to this, detailed information about the sensor aperture size was not available for all radiometers used in this study. Some manufacturers do not provide such specifications, and direct measurement was not feasible without compromising the integrity of the devices. This lack of information limits the ability to quantitatively assess the extent of geometric mismatch. Finally, the relatively small number of measurements per condition should be highlighted ( $n = 3$ ), which may reduce the statistical power for detecting subtle differences.

Future studies should explore a wider variety of LED units and portable radiometers, as both are essential tools to guarantee the correct functioning of photopolymerization units in clinical practice. Additional parameters should be considered, such as curing time, total energy output, and depth of cure, as all are essential for ensuring effective and predictable photopolymerization in clinical practice.

## 5. Conclusions

The results of this in vitro study demonstrate that irradiance values vary significantly depending on the radiometer used, even when evaluating the same light-curing unit under standardized conditions. These discrepancies may affect clinical decisions related to exposure time and material polymerization, emphasizing the need for careful device selection and consistent monitoring.

Clinicians are encouraged to periodically verify the performance of their light-curing units using reliable radiometers—preferably those with proven accuracy—and to document irradiance values over time. Although portable radiometers have limitations, they remain valuable tools for identifying performance changes and ensuring effective clinical outcomes.

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